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(\$4) Title: BIOERODIBLE POLYMERS USEFUL F	FOR T	E CONTROLLED RELEASE OF THERAPEUTIC AGENTS
Bioerodible ortho ester polymers useful for prements, creams, gels and the like are provided. A novel	synthe	oft form bioerodible pharmaceutical compositions such as oint- method for preparing the polymers is provided as well. Synthesis and a triol. The pharmaceutical compositions of the invention are

involves a une-step reaction netwern a monoment or no ester and a triol. Interpharmaceutical compositions of the invention are useful for the controlled release of therapeutic agents, and may be administered for a variety of purposes, such as for the treatment of deep wounds, including burns, and for the treatment of periodontal disease.

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BIOERODIBLE POLYMERS USEFUL FOR THE CONTROLLED RELEASE OF THERAPEUTIC AGENTS

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Description

15 Technical Field

The present invention is in the fields of polymer chemistry and drug delivery, and it concerns certain ortho ester polymers and methods for their preparation. These materials are bioerodible polymers,

- 20 i.e., polymers containing hydrolytically labile linkages which undergo cleavage at physiologic conditions. These bioerodible polymers are useful for the controlled release of therapeutic agents. Thus, the invention relates to drug dosage forms prepared with the novel polymers,
- 25 including solid implantable drug dosage forms as well as soft forms, such as ointments, gels, creams and the like. The invention additionally relates to the use of these bioerodible drug dosage forms and the treatment of disease conditions such as deep wounds, periodontal disease, and
- 30 the like.

Background

Bioerodible polymers used to control the release of therapeutic agents physically dispersed in the polymer matrix have been described in a variety of contexts. One matrix which has been successful is a family of poly(ortho

esters). These materials contain the pH-sensitive ortho ester linkage in their polymer backbone. Such polymers are described, for example, in U.S. Patent No. 4,304,767 to Heller et al. Because the ortho ester linkages within 5 these polymers are relatively stable at neutral pH, and hydrolyze progressively faster with the decreasing pH of the surrounding medium, the rate of erosion of the polymer can be manipulated within a very wide range by incorporating various levels and strengths of acidic excipients into 10 the polymer matrix.

The method of preparing polymers according to the aforementioned patent comprises the addition of polyols to diketene acetals as shown in Scheme 1.

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Using this scheme, almost any diketene acetal and any diol can be used, and the synthetic method is thus extremely versatile. Polymers synthesized by this method are, however, not optimal for preparing soft or amorphous drug dosage forms such as bioerodible ointments, creams or gels due to the relatively rigid pentaerythritol segment in the polymer backbone.

There is a need in the art for a bioerodible composition which has a molecular structure of sufficient 10 flexibility to enable its use as a bioerodible matrix in soft dosage forms such as ointments, gels, creams, or the like. An ideal material would enable the topical delivery of an effective dose level of pharmaceutical agent from an ointment or the like at a desired rate for a period of time dictated only by clinical considerations and not by

limitations of the ointment cream or gel formulation. The ability to achieve this is particularly important in cases where excessive and uncontrolled application of a drug can produce serious side effects.

The present invention is addressed to these considerations, and provides bioerodible compositions which may be prepared in either solid implantable forms or in soft dosage forms such as ointments or the like, as noted above. In these bioerodible drug dosage forms, the 25 release rate of the drug to be delivered—as well as the desired time period for drug delivery—can be carefully controlled. It provides materials which bioerode to small, water—soluble molecules that leave no residues in the tissue of the patient undergoing treatment. This 30 opens the door for improved treatment of burns, wounds, especially deep wounds, and like applications by the

controlled delivery of drugs over prolonged periods of

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time.

Disclosure of the Invention

It is accordingly a primary object of the present invention to address the aforementioned needs in the art, and to provide bioerodible compositions useful in 5 either solid implantable or soft dosage forms for the controlled release of therapeutic agents.

It is another object of the invention to provide these bioerodible compositions in the form of bioerodible solid implants.

10 It is still another object of the invention to provide these bioerodible compositions in the form of bioerodible ointments, gels, creams or the like.

Is it yet another object of the invention to provide a novel method of synthesizing certain bioerodible 15 ortho ester polymers useful for such compositions, as well as certain novel bioerodible ortho ester polymers themselves.

It is a further object of the invention to provide a bioerodible ointment and method for the treat20 ment of deep wounds, periodontal disease, and the like.

These objects are achieved by the present invention. In accord with this invention, a method is provided for synthesizing a bioerodible ortho ester polymer. This method involves:

25 reacting a monomeric ortho ester having the general formula

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wherein R is hydrogen or an alkyl of 1 to 10 carbon atoms and R' is a lower alkyl of 1 to 6 carbon atoms, with a triol having the general formula

WO 91/03510

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wherein A is alkylene or cycloalkylene of at least 5 carbon atoms, or an oxyalkylene of at least 5 carbons and having its oxygen as an ether linkage, e.g., within a saccharide structure. This reaction forms an ortho ester polymer containing a mer unit having the following general formula (I)

ortho ester polymer is another aspect of this invention.

In another aspect of the present invention, bioerodible pharmaceutical compositions are provided based on these ortho ester polymers. These compositions are either in solid implantable form or in a soft dosage form, and contain one or more of these bioerodible ortho ester polymers and an effective amount of a selected therapeutic agent. This aspect of the invention also relates to a method for the prolonged treatment of disease states in man and animals such as treating burns, deep wounds, and the like. This method comprises either administering topically to such a patient a pharmaceutical ointment,

15 wherein the A and R units are as just described. This

30 of the ortho ester polymer and the gradual exposure and controlled delivery of the therapeutic agent.

gel, cream, or the like, or implanting a solid formulation of this invention and thus achieving controlled bioerosion

Brief Description of the Drawing

Figure 1 is a graph illustrating the effect of 35 an acidic excipient on the rate of bioerosion of the ortho-ester-based compositions of this invention.

Detailed Description of the Invention

A. Definitions

The term "mer" is used to mean the structurally
5 recurring units or monomer units of the ortho ester
polymers provided by the present invention. The mer units
of any given polymer may be the same or different; when
different, they may be arranged in block or random
fashion. When all the mer units of a polymer are the
10 same, the polymer is called a homopolymer. When there are

2 or more mer units in a polymer, the polymer is called a copolymer. The present invention involves both homopolymers and copolymers.

The term "bioerodible" as used herein to

15 describe the polymers of the present invention is
synonymous with the term of art "biodegradable." These
terms denote the property of a body of solid gel polymer
to undergo degradation, erosion and solubilization as a
result of hydrolysis of labile linkages at the physiologic
20 conditions of use.

The terms "therapeutic agent" or "drug" are used interchangeably to mean a compound or composition of matter which, when administered to an organism (human or animal) induces a desired pharmacologic and/or physiologic

25 effect by local and/or systemic action. In general, the terms include the therapeutic or prophylactic agents in all major therapeutic/prophylactic areas of medicine. The term "effective amount" as used herein

intends that quantity of a therapeutic agent that, when administered to a patient, is required to provide the desired or intended beneficial effect without intolerable side effects, such as toxicity. When used in the context of controlled delivery or prolonged delivery of drug, the term can include a temporal aspect—noting that the <u>rate</u>

35 of administration gives the desired effect without intolerable side effects.

-7-

The term "soft dosage form" as used herein is intended to mean a bioerodible ointment, gel, cream or the like, typically intended for topical administration of a drug.

The term "implantable" drug dosage form as used herein is intended to mean a drug-bearing polymeric body designed to be implanted subcutaneously or in a body cavity so as to give rise to sustained release of the contained drug.

The term 'lower alkyl' is intended to mean linear, branched or cyclic alkyl moieties having 1 to 6, and more typically 1-5 carbon atoms, inclusive.

The terms "alkylene" and "cycloalkylene" have their usual meaning defining aliphatic linking groups, 15 preferably aliphatic hydrocarbon groups which serve as a

The term "oxyalkylene" defines an aliphatic linking group containing 1 or more ether oxygens and providing 2 or more carbons as bridge points to other 20 groups. Oxyalkylene groups can be linear, branched or cyclic.

bridge between 2 or more other groups.

B. Synthetic Method

In the synthesis aspects of the present inven25 tion, a method is provided for synthesizing certain
bioerodible ortho ester polymers. The synthesis is a
simple, straightforward reaction which may be accomplished
in one step in a single reaction vessel. The synthesis
involves the reaction of a monomeric ortho ester having
30 the general formula

wherein R is a hydrogen or an alkyl of 1 to 10 carbon atoms and each of the Rs is independently selected from lower alkyls, with a triol having the general formula

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In this triol, A is an alkylene or a cycloalkylene moiety of 5 carbon atoms or more, or is an oxyalkylene. If cycloalkylene or a cyclic oxyalkylene, A will preferably contain 1 to 3, more preferably 1 or 2, rings. The reaction is carried out to form an ortho ester polymer which comprises mer units of the structure (I)

$$R$$
 O A (1)

In preferred embodiments, the R moiety of the 20 monomeric ortho ester reactant is lower alkyl, and the R' moieties are the same alkyl, either methyl or ethyl. In preferred embodiments, the triol reactant, the A moiety, is either alkylene or cycloalkylene or oxyalkylene of 5 25 carbon atoms or more, preferably 5 to 20 carbon atoms, and more preferably 5 to 10 carbon atoms. It is preferred that 2 of the hydroxyl groups of the triol be separated by either 2 or 3 carbon atoms (i.e., so that x in the below structures is 0 or 1, respectively), to enable ring forma-30 tion during polymerization, while the third hydroxyl group is preferably separated from the closer of the first 2 hydroxyl groups by 3 carbon atoms or more, (i.e., so that in the below structures y is greater than or equal to 2). This spacing of the third hydroxyl unit will prevent interference with the ring-forming reaction. Thus, in one 10

group of preferred triols, A is a linear alkylene moiety, i.e., having the structure

so that the triol has the structure

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30 Compounds containing analogous substituted pentafuranose rings are within the purview of the present invention as well.

Examples of other cyclooxyalkylene moieties include:

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10 The synthesis reaction of the ortho ester monomer and triol is carried out either neat or in an aprotic solvent such as tetrahydrofuran (THF), cyclohexane, ethylene glycol dimethyl ether (glyme), diglyme, cymene, cumene, 15 chlorinated hydrocarbons, or the like. More typically, solvent is present. Typical concentrations of the two reactants can range from essentially 100% (neat) down through about 10% by weight or lower, when solvent is used. In either case, care must be taken to maintain 20 anhydrous conditions. The reaction can be carried out at reflux and thus, depending upon the solvent, at temperatures in the range of 50-150°C, preferably 50-90°C. The approximate molar ratio of reactants set at about 1:1 if it is desired to maximize the molecular weight of the 25 polymer, but can be varied if a lower molecular weight polymer is desired (e.g., to make a less viscous ointment). It is typically preferred to carry out the reaction in the presence of an acid catalyst, although in cases where the reactants are acidic, a catalyst is un-30 necessary. Examples of suitable acid catalysts include ptoluenesulfonic acid and methanesulfonic acid. The amount of acid catalyst can range from 0% (based on its optional presence) to about 1% molar (based on the amount of triol

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present).

-11-

C. The Novel Bioerodible Polymers

The novel ortho ester polymers useful in the drug dosage forms provided herein preferably contain mer units represented by Formula (I) wherein

(I)

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R is hydrogen or an alkyl of 1 to 10 carbon atoms, preferably a lower alkyl; and A is a cycloalkylene of at least 5 carbon atoms, a cyclooxyalkylene of at least 5 carbon 15 atoms (as in the pentafuranose ring and other cyclooxyalkylene structures illustrated above), or a linear or branched alkylene moiety of at least 5 carbon

atoms given by the structure

In this latter structure, the R" moieties are independently selected from the group consisting of hydrogen and the lower alkyls, x is 0 or 1, and y is an integer greater 25 than or equal to 3.

Typically, although not necessarily, the polymers of the invention have molecular weights ranging from several (2-3) thousand to 10,000-15,000, but can have molecular weights as low as 500 or as high as 50,000 or 30 more. The number of mer units in the polymer, corres-

pondingly, will be between about 5 and 1000, more typically between about 5 and 500, most typically between about 5 and 150.

These polymers have the desirable properties of 35 being able to undergo bioerosion and of being less rigid and more flexible and conforming than prior ortho ester polymers.

C. Pharmaceutical Compositions

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The pharmaceutical compositions of this invention comprise a selected therapeutic agent or number of agents dispersed in a novel bioerodible ortho ester polymer as described in the preceding section. While the preferred pharmaceutical compositions of the invention 10 include solid implantable drug dosage forms and soft dosage forms such as bioerodible ointments, gels and creams, it is intended that other drug dosage forms and other modes of administration (e.g., transdermal, transmucosal, intraocular, etc.) be within the scope of the invention as 15 well.

The bioerodible ointments, gels and creams of the invention will include: an ointment, gel or cream base comprising one or more of the bioerodible ortho ester polymers described herein and a selected therapeutic 20 agent. The therapeutic against, whether present as a liquid, a finely divided solid, or any other physical form, is dispersed in the ointment, gel or cream base. Typically, but optionally, the compositions include one or more other components, e.g., nontoxic auxiliary substances 25 such as colorants, diluents, odorants, carriers, excipients, stabilizers or the like.

For solid compositions, conventional nontoxic solid carriers include, for example, pharmaceutical grades of mannitol, lactose, starch, magnesium stearate, sodium 30 saccharin, talcum, cellulose, glucose, sucrose, magnesium carbonate, and the like. The solid implantable formulation to be administered will contain a quantity of active compound or compounds in an amount effective to alleviate the symptoms of the subject being treated.

35 The amount of active agent will be dependent upon the particular drug employed and condition being

treated. Typically the amount of drug represents about 0.001% to about 70%, more typically about 0.001% to about 50%, most typically about 0.001% to about 20% by weight of the total composition being common.

5 The quantity and type of ortho ester polymer incorporated into the implant, ointment, gel, cream, etc., is variable. For a more viscous composition, a higher molecular weight polymer is used. If a less viscous composition is desired, a lower molecular weight polymer 10 can be employed, i.e., one which is prepared with other

than a 1:1 reactant ratio. The product may be based on only one polymer or it may comprise a mixture of polymers.

While not essential for topical or transdermal administration of many drugs, it may in some cases, with

15 some drugs, be preferred that a skin permeation enhancer be coadministered therewith. Any number of the many skin permeation enhancers known in the art may be used. Examples of suitable enhancers include dimethylsulfoxide (DMSO), dimethylformamide (DMF), N, N-dimethylacetemide 20 (DMA), desylmethylsulfoxide (C10MSO), ethanol, eucalyptol,

lecithin, and the 1-N-dodecylcyclazacycloheptan-2-ones (available under the trademark Azone from the Nelson Research and Development Company, Irvine, California).

It is additionally preferred to incorporate an 25 acidic excipient into the bioerodible dosage form in order to control the rate of polymer bioerosion. The ortho ester linkages of the bioerodible polymers are relatively stable at basic or neutral pH and are hydrolized at progressively increasing rates as the pH of the medium

30 surrounding the polymer decreases. Thus, hydrolytic lability and the rate of erosion and drug release can be increased by incorporation of one or more acidic components. Preferred acidic excipients are aliphatic acids, typically present at 0-10 wt%, more preferably

35 1-5 wt%, of the bioerodible composition. Solid but water soluble aliphatic acids are generally favored. Examples of acidic excipients useful in conjunction with the present invention include adipic, citric, suberic; maleic and itaconic acids. Basic excipients may also be used to slow the rate of release.

The variety of different therapeutic agents which can be used in conjunction with the bioerodible compositions of the invention is vast. In general, therapeutic agents which may be administered via the pharmaceutical compositions of the invention include, 10 without limitation: antiinfectives such as antibiotics and antiviral agents; analgesics and analgesic combinations; anorexics; antihelminthics; antiarthritics; antiasthmatic agents; anticonvulsants; antidepressants; antidiabetic agents; antidiarrheals; antihistamines; 15 antiinflammatory agents; antimigraine preparations; antinauseants; antineoplastics; antiparkinsonism drugs; antipruritics; antipsychotics; antipyretics; antispasmodics; anticholinergics; sympathomimetics; xanthine derivatives; cardiovascular preparations includ-20 ing calcium channel blockers and beta-blockers such as pindolol and antiarrythmics; antihypertensives; diuretics; vasodilators including general coronary, peripheral and cerebral; central nervous system stimulants; cough and cold preparations, including decongestants; hormones such 25 as estradiol and other steroids, including corticosteroids: hypnotics: immunosuppressives; muscle relaxants; parasympatholytics; psychostimulants;

In particularly preferred embodiments, the 30 therapeutic agents for administration in conjunction with the bioerodible polymers of the invention are antibacterial agents for the treatment of deep wounds, antibiotics (e.g., tetracycline or the like) for periodontal treatment or subcutaneous/subgingival abscesses, antiinflammatory

35 agents (e.g., meclofenamate sodium, oxyphenbutazone, indomethacin, mefenamic acid, ibuprofen and naproxen,

sedatives: and tranquilizers.

etc.), antibiotics and adrenal corticosteroids for use in intraarticular injection or implantation, intraocular/ orbital adrenal corticosteroids, antiviral agents or antibiotics, and antihypertensive agents (e.g., hydralazine, minoxidil or the like). Other preferred drugs for use with the presently disclosed polymers include proteinaceous drugs such as epidermal growth factors or growth hormones.

The present invention also encompasses

10 veterinary applications of the presently disclosed
polymers, pharmaceutical compositions, and methods of
treatment.

D. Administration and Use

15 Depending on dosage form, the pharmaceutical compositions of the preceding section may be administered in different ways, i.e., topically, parenterally, or the like. Preferred dosage forms are solid implants or soft dosage forms which can be applied directly to the af-20 flicted tissue for the delivery of drug. The ortho ester polymer, upon contact with body fluids including perspiration, saliva, or the like (depending upon the mode of administration), undergoes gradual bioerosion with concomitant gradual exposure of the dispersed drug to the 25 afflicted tissue. This can result in prolonged delivery (over, say, 1 to 10,000 hours, preferably 2 to 1000 hours) of effective amounts (say, 0.0001 mg/kg/hour to 10 mg/kg/ hour) of the drug. Application can be repeated as necessary depending on the subject being treated, the severity 30 of the affliction, the judgment of the prescribing physician, and the like. Topical application can be enhanced by occlusion, i.e., placing a barrier over the area treated so as to enhance absorption into the skin. Topical administration or implantation is preferred for

35 wound healing and in the treatment of periodontal disease.

Parenteral administration of a bioerodible composition of the invention can be effected by either subcutaneous or intramuscular injection. The bioerodible ointment, gel or cream may be injected as is or in 5 combination with one or more auxiliary components as described above. Parenteral delivery is preferred for administration of proteinaceous drugs such as growth factors, growth hormone, or the like.

Intraocular, transdermal or transmucosal
10 administration of bioerodible compositions of the invention can also be carried out according to conventional
means.

Examples

The examples presented below are provided as a further guide to the practitioner of ordinary skill in the art, and are not to be construed as limiting the invention in any way.

20 Example 1

Under anhydrous conditions, 48.669 q (0.30 moles) of triethylorthoacetate, 40.25 g (0.30 moles) of 1,2,6-hexanetriol and 20 mg of p-toluenesulfonic acid were weighed into a 500 ml round bottom flask equipped with a 25 magnetic stirring bar. To the flask was added 300 ml cyclohexane and the flask was adapted to a 60 cm spinning band column. The reaction flask was heated at 100°C with vigorous stirring and the distillate, which included an azeotrope of by-product and cyclohexane ethanol, was 30 removed rapidly at 65°C while a strictly anhydrous condition was maintained. As the boiling point started to climb beyond 65°C, the distillation rate was reduced to 1/ 20 (distillation/reflux ratio) until the boiling point reached 81°C. Then the column was set at that total 35 reflux. After heating for an additional 4 hours, the solution was cooled to room temperature. Five drops of

-17-

triethylamine were added and solvent was removed by evaporation. The product was a viscous liquid having a weight average molecular weight (MW) of 29,000 as determined by GPC.

Example 2

Following the procedure as described in Example 1, 52.878 g (0.30 mole) of triethylorthopropionate was reacted with 40.25 g (0.30 mole) of 1,2,6-hexanetriol.

10 The by-product ethanol was removed by azeotropic distilla-

The by-product ethanol was removed by azeotropic distilla tion with cyclohexane to yield a polymer having a MW of 19,300.

Example 3

15 Following the procedure as presented in Example 1, 14.82 g (0.10 mole) of trimethylorthobutyrate was reacted with 13.42 g (0.10 mole). The by-product methanol was removed by azeotropic distillation with cyclohexane from 54°C to 81°C to yield a polymer having a MW of 20 27.600.

Example 4

Following the procedure as presented in Example 1, 16.223 g (0.10 mole) of triethylothoacetate was 25 reacted with 12.015 g (0.10 mole) of 1,2,5-pentanetriol to yield a polymer having a MW of 25,000.

Example 5

Following the procedure as described in Example 30 1, 3.82 g (31.74 mmoles) of trimethyl orthoacetate was reacted with 4.64 g (31.74 mmoles) of cis-3,4-dihydroxycyclohexanemethanol. The by-product methanol was removed by azeotropic distillation with cyclohexane. After evaporation of the cyclohexane, the polymer was 35 redissolved in tetrahydrofuran and precipitated into a large excess of methanol containing a small amount of

triethylamine stabilizer. The solid polymer, isolated by filtration, had a molecular weight ($\rm M_{c})$ of 25,000.

The monomer was prepared as follows:

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Example 6

A bioerodible ointment was prepared with 2 wt% hydrocortisone physically dispersed in a soft, bioerodible ortho ester polymer having the structure

synthesized using the methods described in the preceding examples. To demonstrate bioerodibility, a body of this ointment was exposed to a slow (9 mm/min) flow of buffer 10 solution, pH 7.4. Fractions were collected and the ap-

pearance of the drug in the collected buffer was analyzed by HPLC. Because hydrolysis of orthoester linkages at pH 7.4 is very slow, no hydrocortisone was released in the absence of an incorporated acidic excipient. Upon in-

15 corporation of 2 wt% of adipic acid into the bioerodible ointment, bioerosion took place and hydrocortisone was released. Results are summarized graphically in Figure 1. The rate of hydrocortisone release can thus be controlled by the amount of the incorporated acidic excipient or the 20 use of materials having varying acidity.

Example 7

A bioexodible, 20 mm x 2 mm cylindrical implant was fabricated by first dissolving the polymer of 25 Example 5 in tetrahydrofuran and then adding to the viscous polymer solution 10 wt% (based on polymer weight) of the anticancer agent 5-fluorouracil. After solvent evaporation, devices were fabricated by transfer molding. To demonstrate bioexodibility, the cylindrical devices 30 were exposed to a slow (9 cc/min) flow of buffer solution, pH 7.4, at 37°C. Fractions were collected, and the appearance of 5-fluorouracil in the collected buffer was analyzed by HFLC. Because hydrolysis of the polymer at pH 7.4 is very slow, no drug was released in the absence of

35 an acidic excipient. Upon incorporation of 1 wt% suberic acid, bioerosion took place and 5-fluorouracil was WO 91/03510

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released. The rate of drug release can thus be controlled by the amount and acidity of the incorporated acidic excipient.

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-21-

WHAT IS CLAIMED IS:

 $\mbox{1.} \quad \mbox{$A$ method for preparing a bioerodible polymer comprising:}$

5 reacting a monomeric ortho ester having the general formula

OR' R-C-O

wherein R is hydrogen or alkyl or 1 to 10 carbon atoms and R' is lower alkyl, with a triol having the general formula 15

wherein A is selected from alkylenes and cycloalkylenes of 20 at least 5 carbon atoms, and oxyalkylenes and cyclooxyalkylenes of at least 5 carbons, to form a nonrigid, bioerodible ortho ester polymer comprising mer units of the structure

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 The method of claim 1 wherein R is hydrogen or lower alkyl.

3. The method of claim 1 wherein A is an alkylene of from about 5 to about 20 carbon atoms.

- 4. The method of claim 1 wherein A is a cycloalkylene moiety of from about 5 to 20 carbon atoms.
- The method of claim 1 wherein A is a 5 cyclooxyalkylene moiety of from about 5 to about 20 carbon atoms.
 - $\mbox{6. The method of claim 5 wherein said triol is a sugar residue. } \\$

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7. The method of claim 1 wherein A has the general formula:

15

wherein x is 0 or 1, y is greater than or equal to 2, and the R"s are independently selected from the group consisting of hydrogen and lower alkyl.

- 20 8. The method of claim 7 wherein x is 0, y is 4 and the R's are each hydrogen.
- The method of claim 1 wherein the number of mer units in the final polymer is in the range of about 5 to about 1000.
 - 10. A polymer containing repeating mer units of the structure

30

$$\begin{pmatrix} R & O \\ O & A \end{pmatrix}$$

35 wherein R is hydrogen or alkyl of 1 to 10 carbon atoms and A is selected from the group consisting of cycloalkylenes

of at least 5 carbon atoms, cyclooxyalkylenes of at least 5 carbon atoms, and alkylenes having the structure

$$CR"_2$$
 $-(CR"_2)_x$ $-CR"$ $-(CR"_2)_y$ $-$

wherein x is 0 or 1, y is greater than or equal to 3, and the R"s are independently selected from the group consisting of hydrogen and lower alkyl.

- 10 11. The polymer of claim 10 wherein A is cycloalkylene of about 5 to 20 carbon atoms.
- 12. The polymer of claim 11 wherein A is cycloalkylenes of about 5 to 10 carbon atoms.
 15
 - 13. The polymer of claim 10 wherein A is a cyclooxyalkylene and comprises a pentafuranose ring.
- \$14.\$ The polymer of claim 10 wherein R is 20 hydrogen or lower alkyl.
 - \$15.\$ The polymer of claim 13 wherein R is hydrogen or lower alkyl.
- 25 16. The polymer of claim 10 having a molecular weight of at least about 500.
 - 17. The polymer of claim 10 having a molecular weight of at least about 2,000.

- $\ensuremath{19}$. The composition of claim 18 further comprising an added acid.
- \$20.\$ the composition of claim 18 in the form of 5 an ointment.
 - 21. The composition of claim 18 in the form of a cream.
- 10 22. The composition of claim 18 in the form of a solid implant.
- 23. The composition of claim 18 wherein the therapeutic agent is a proteinaceous drug.
 15
- 24. The composition of claim 18 wherein the therapeutic agent is selected from the group consisting of antibacterial agents, antibiotics, antiinflammatory agents, antihypertensive agents, antiviral agents and 20 adrenal corticosteroids.

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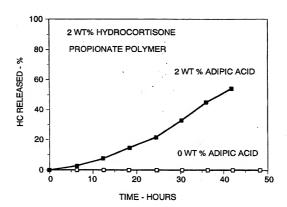


FIG. 1

INTERNATIONAL SEARCH REPORT

	INTERNATIONAL S			
	CIFICATION OF CURITOR WARRES		T/US90/04804	
Account	SIFICATION OF SUBJECT MATTER IN Several classific g to International Patent Classification (IPC) or to ooth Natio	cition symbols apply, indicate all)		
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III. DOC	UMENTS CONSIDERED TO BE RELEVANT .			
ategory *	Citetian of Document, " with indication where appro-	corrate, of the reterant cessages '2	Relevent to Claim No '3	
A	US, A, 4,066,747 (CAPOZZA)	03 JANUARY 1978		
A	US, A, 4,079,038 (CHOI) 14	MARCH 1978		
A	US, A, 4,119,579 (CAPOZZA)	10 OCTOBER 1978		
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		"X" occument of particular reference; the cleimed " cennot be considered novel or cannot be corsidered."		
			"Y" oncument of netticular relevance: the claimed "	
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"P" d	ocument aublished orior to the internetional filing date but ter than the oriority dete Cleimed	"A" accument memoer of the same	e patent family	
	TIFICATION .			
Date of	ine Actual Completion of the International Search	0 7 JAN 199	Search Report	
	26 OCTOBER 1990	Superior of Autograph Off		
internati	onal Searching Authority	Signature of Authorities Office	_	
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